

# Chapter 2

## Mathematical-Computational Simulation of Cytoskeletal Dynamics

Carlos A. de Moura, Mauricio V. Kritz, Thiago F. Leal, and Andreas Prokop

**Abstract** Actin and microtubules are components of the cytoskeleton, and are key mediators of neuron growth and maintenance. Knowing how they are regulated enhances our understanding of neural development, ageing, degeneration, and regeneration. However, biological investigation alone will not unravel the complex cytoskeletal machinery. We expect that inquiries about the cytoskeleton can be significantly enhanced if their physico-chemical behavior is concealed and summarized in mathematical and computational models that can be coupled to concepts of biological regulation. Our computational modeling concerns the mechanical aspects associated with the dynamics of relatively simple, finger-like membrane protrusions called filopodia. Here we propose an alternative approach for representing the displacement of molecules and cytoplasmic fluid in the extremely narrow and long filopodia and discuss strategies to couple the particle-in-cell method with algorithms for laminar flow to model the two phases of actin dynamics: polymerization into filaments which are pulled back into the cell and compensatory G-actin drift towards its tip to supply polymerization. We use nerve cells of the fruit fly *Drosophila* as an effective, genetically amenable biological system to generate experimental data as the basis for the abstract models and their validation.

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## 2.1 Introduction

Biological phenomena rely on physical and chemical interactions. As elements of a physical phenomenon, biological components interact freely with one another: whenever in contact they exchange mass and energy. Their interactions as chemical elements are not as free, since they depend on chemical compatibilities of the interacting elements. This makes biological interactions highly complex. The elements giving cause to biological phenomena are dynamic, self-regulatory, and resilient, and entities often interact through the exchange of information (signals), without being necessarily in contact or even close together.

To understand biological systems at the sub-cellular scale, we need to disentangle the organizational (functional) status of biological elements, as well as the regulatory elements, interactions, and rules underlying their dynamics, from purely biochemical reactions. All biological processes are grounded on physical and chemical interactions but some of them have only sense within cells or other organisms, having no reason to spontaneously exist elsewhere.

A way to achieve this is to have the physico-chemical dynamics well described and operationally documented as a working and consensual mathematical/computational model amenable to manipulations at higher levels, including by regulatory mechanisms induced by signaling and other stimuli. This can be achieved through the employment of mathematics and computer science to represent the behavior of complex systems occurring in life-phenomena, through structured algorithm-based simulations [6, 11, 24, 25, 37]. The key purpose is to represent or reproduce properties that the system under analysis displays.

Both types of observation, real experimental data and computer simulation, complement each other in several ways. Computational modeling depends on data, insights and concepts/cartoon models derived from real experimentation (in our case with biological systems). Vice versa, mathematical/computational models offer several advantages to advance the understanding of biological systems: (a) they offer inclusion of wider ranges of parameters far beyond the capacity of the human mind, (b) they can operate beyond space and time scales that can be experimentally addressed, (c) allow variables and geometries to be easily adjusted to study their impacts on the system, (d) make predictions or suggest the existence of particular interactions or structures that can then be tested experimentally, (e) provide opportunities to test assumptions and theoretical knowledge in order to refine hypotheses or suggest what might be true, (f) determine which experimental variables are most important in a system, and (g) can be used to synthesize experimental data and for testing data interpretation methods. The Nobel Prize winning physicist Kenneth Wilson proposed in the late 1980s that, for different sciences, computational modeling ought to gain the same status as theoretical

analyses and laboratory experiments [59]. This enlarges the possibilities inherent in the scientific hypothesis-deduction-observation cycle and relaxes the constraints imposed by the impossibility of performing certain experiments.

We aim to model biological problems and, for this, we focus on the cytoskeleton. The cytoskeleton comprises mechano-resistant, yet highly dynamic, networks composed of filamentous protein polymers, called actin (thin filaments; diameter of 5–7 nm), intermediate filaments (5–12 nm), and microtubules (thick filaments; ~25 nm), which support cell architecture and dynamics [20]. There is virtually no cell function that does not depend on the cytoskeleton, yet the number of essential proteins binding and regulating the cytoskeleton is surprisingly low [15, 49]. This is possible because the same cytoskeletal regulating proteins can be employed in different contexts, contributing to very distinct cytoskeletal networks and dynamics. Therefore, genetic defects of any of these components will have multiple (pleiotropic) effects, and the many human diseases caused by such defects [49] are by nature complex systemic phenomena. Furthermore, cytoskeletal dynamics are the cause and consequence of both chemical interactions and physical forces, and its analysis requires thinking at the interface of biochemistry and biomechanics [7].

In this chapter, we discuss a new approach to model cytoskeletal dynamics by focussing on the relatively simple context of filopodia. Filopodia are long finger-like membrane protrusions which act as tentacle-like sensors receiving signals as well as active devices that contact other cells to convey signals. The essential architectural feature of filopodia are parallel, cross-linked bundles of actin filaments which are pulled back into the cell through disassembly processes at their base, compensated for by extensive polymerization at the very tip. This leads to a continuous treadmill-like turnover of these actin filaments. By adjusting the proportion of the polar assembly versus disassembly processes, filopodia can undergo regulated length changes. However, the high rate of polymerization at the very tip of filopodia requires uninterrupted delivery of large amounts of new building blocks which, at first sight, seems counterintuitive in these long and slender protrusions [19, 22, 31, 33]. To explain this phenomenon, we propose the use of integrative models which consider catalyzed actin polymerization dynamics, diffusion as well as cytoplasmic flow dynamics.

## 2.2 The Object of Our Study

### 2.2.1 *Actin Dynamics*

Actin is the most abundant protein in eukaryotic cells [47]. Actin exists as globular actin monomers called G-actin and polar filaments called F-actin. Actin filaments are head-to-tail polymers of G-actin subunits. The minus, or pointed, end of actin filaments is relatively inert displaying slow growth *in vitro*. The opposite plus, or barbed, end grows much faster through exothermic polymerization both *in vitro* and *in vivo* [9].



another by a range of different cross-linking proteins or myosin motor proteins; stabilizing filaments, weaving them into different classes of networks, using them as highways for transport processes or as scaffolds to pull and generate forces [7, 38].

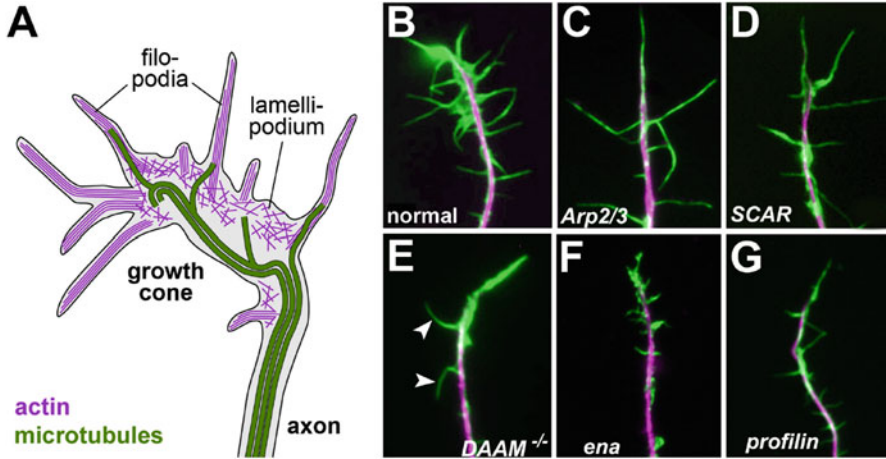
Of particular importance for this chapter is the plus-end polymerization of actin. It occurs through intermolecular associations that depend on the special organization and molecular structure of the intervening monomers. Actin polymerization in cells is regulated by a number of proteins that bind G-actin and/or the actins at the plus-ends of the filaments. Amongst these, Ena/VASP, formins, profilin, and capping proteins are particularly important (Fig. 2.1). Capping proteins, such as CapZs or adducin, bind and stabilize the F-actin plus-end, i.e., suppress polymerization [1, 16].

Profilin binds and sequesters G-actin and is therefore, by default, an inhibitor of nucleation and enhancer of depolymerization [5]. However, this role changes dramatically if formins or Ena/VASP are present and bound to the elongating plus-ends. These proteins bind profilin-actin with high affinity and utilize it as G-actin source to catalyze and actively promote plus-end polymerization [3, 8]. In addition, they out-compete capping proteins, and Ena/Vasp can bundle the plus-ends of F-actin as well as position it at the membrane [3]. Therefore, apart from the physical properties of actin and its polymerization processes, the biochemical contributions of these actin regulators need to be considered in any models aiming to describe actin dynamics.

## 2.2.2 *Filopodia*

Filopodia are relatively simple cellular compartments providing a realistic context in which to start modeling the complexity of actin network regulation in biological contexts. Filopodia are long, finger-like membrane protrusions with numerous roles in signaling and cell navigation (Fig. 2.2a) [19, 22, 31, 33]. Unlike the enormous complexity of most cellular regions with dynamically interchanging actin networks, the comparatively simple organization of filopodia offers great advantages: (1) they contain only one form of prevailing actin network consisting of parallel F-actin bundles; (2) accordingly, the number of molecular players is limited; (3) filopodial dynamics are predominantly unidimensional, and (4) length changes of filopodial actin filament bundles directly translate into length changes of the entire filopodium, thus providing simple and efficient readouts for functional studies that can be carried out iteratively with modeling approaches (Fig. 2.2b–g) [44].

Therefore, the regulation of filopodial dynamics appears relatively simple, essentially governed by the proteins regulating polymerization and disassembly processes. The key challenge in understanding filopodial dynamics is the high rate of polymerization at the very tip, which requires constant delivery of actin monomers through these slender and long structures. Therefore, how polymerization can be sustained within the highly challenging filopodial structure is a fascinating phenomenon which harbors key explanations for filopodial behaviors. Any models



**Fig. 2.2** Growth cone morphology. (a) A growth cone showing bundles of F-actin in filopodia and lattices in lamellipodia (taken from [55]). (b–g) Growth cones of fly neurons in culture lacking specific actin regulators which affect nucleation (c–e) leading to reduced filopodia number but not length, or polymerization (f, g) primarily affecting filopodial length (modified from [44])

of this process will have to consider that most G-actin is likely bound to profilin which will change its diffusion properties and enormously facilitate polymerization at the plus-end [3] where concentrations of G-actin can be expected to be very low. In support of this assumption, formins and Ena/VASP as active polymerizers and interactors of profilin are concentrated at filopodial tips, and deficiencies of profilin or Ena/VASP cause dramatic shortening of filopodia [44].

### 2.3 Suitable Biological Systems for Parallel Experimental Approaches

A key prerequisite for successful modeling is the existence of biological data and concepts/cartoon models. Since there is no single cellular system used in biological research which would alone provide sufficient insights and experimental data, the only feasible strategy to develop conceptual cartoon models for filopodial dynamics is to integrate mechanistic conclusions obtained from a wide range of very different cellular systems [19, 22, 31, 33]. However, this approach can be misleading since properties of filopodia may vary between animal species and cell types. Ideally, one would want a single and standardized experimental system so that data and mechanistic concepts can be reliably integrated. This would enormously facilitate the experimental validation of predictions made from mathematical modeling, especially if these predictions concern the interface between different parameters or elements.

As biological systems suitable for studying filopodia, growth cones are particularly well suited since they are rich in actin networks and reliably display filopodia as a prominent and functionally important structural feature (Fig. 2.2) [14, 23]. Growth cones are the motile tips of growing axons, the long and slender processes of nerve cells which form the cables that wire the nervous system. To lay these cables during development or regeneration, the growth cones at their tips navigate along specified paths, and their prominent filopodia act as sensors facilitating proper navigation [55]. Apart from the fact that growth cones display prominent filopodia with a clearly defined function, there is a good conceptual understanding of the fundamental roles that actin plays in growth cones, and their actin machinery is well investigated in this context [23, 41].

More recently, growth cones of the fruit fly *Drosophila* have been established as powerful models accessible to detailed studies of the cytoskeleton and systematic genetic dissections of its various regulators [49, 51, 55, 56]. For example, a systematic study used filopodial number and length as a simple readout to understand the systemic contributions and functional interfaces of seven different actin-binding regulators, which included formins, Ena/VASP, profilin, and capping proteins (Fig. 2.2b–g). This chapter demonstrated how *Drosophila* growth cones can be used to deduce cartoon models of filopodial dynamics [44, 50]. Given the relative speed and ease with which experiments can be carried out in *Drosophila* neurons, this system is ideal for partnering up with the mathematical/computational modeling of filopodial dynamics [49].

## 2.4 Modeling Filopodia

### 2.4.1 Previous Models

Since the end of the 1950s, researchers have been developing models to quantitatively validate experimental results from their laboratory experiments. Very early on, Oosawa and colleagues found that actin polymerization processes were dependent of G-actin concentration [39]. In another early seminal study, Wegner mathematically described actin treadmilling [58]. A further good example is the ordinary differential equation model by Bindschadler and colleagues which explicitly accounts for nucleotide-dependent actin polymerization and depolymerization [4].

At about the same time, taking advantage of technological advance and detailed experimentally measured data, Vavylonis and colleagues built a quantitative discrete model of actin polymerization [57]. This model could be validated by new in vitro experiments using reflection fluorescence microscopy [21]. Mechanisms of actin polymerization have been studied including the interactions between actins and actin-binding proteins (ABPs) and the rate constants for each step leading to quantitative models of polymerization [47].

Another important model that elucidated thinking about how actin polymerization can dynamically control cell shape and motility was the Brownian ratchet model by Peskin and colleagues [43] which aims to explain how chemical reactions generate protrusive forces by rectifying Brownian motion. The ratchet mechanism is the intercalation of monomers between the barrier, (e.g., membrane) and the polymer tip. A particle diffuses in one dimension ahead of a growing bundle of filaments, executing a continuous random walk in a constant force field. As a result, it analyzes polymerization velocity as a function of the load force.

Actin dynamics in motile cells have also been the subject of many modeling approaches. For example, the model by Mogilner and Keshet showed how membrane speed depends on actin monomer concentration and cycle (ATP hydrolysis, F-actin treadmill), reactions with ABPs and barbed end polymerization at the leading edge of a cell [34]. Dawes and colleagues investigated the spatial distribution of actin filaments and their barbed ends, and the interplay between filament branching, growth, and decay at the leading edge [12]. Others investigated the mechanisms of pushing and pulling by actin and microtubules [35], the relations between protrusions, monomer concentration, and stiffness of the filament bundles [36], or anterograde flow of cytoplasm to provide sufficient material for the extension of protrusions, such as lamellipodia [27].

As these examples illustrate, the modeling of actin in biological contexts has to include different levels of resolution, such as structural, physical, and chemical properties of actin filaments and protein complexes that govern F-actin dynamics [7].

With regard to modeling filopodia, several previous attempts should be mentioned. For example, Lan and Papoian used stochastic simulations of filopodial dynamics, discretizing space into compartments, and simulating protein diffusion along the filopodium as a random walk [28]. Erban and colleagues modeled the problem of G-actin delivery to the filopodial tip based on diffusion, 3D stochastic models, and comparing compartmental and molecular models as strategies to simulate actin dynamics [17]. An impressively comprehensive model was published by Mogilner and Rubinstein who included aspects such as physical properties, cross-linkage and numbers of filaments, membrane resistance as well as the G-actin diffusion coefficient [36]. Another recent model by Zhuravlev and colleagues proposed that a key limiting factor of filopodial length is diffusional transport of G-actin monomers to the polymerizing barbed ends, and they investigated potential roles of active motor-driven transport of G-actin [61]. They concluded that “a naive design of molecular-motor-based active transport would almost always be inefficient—an intricately organized kinetic scheme, with finely tuned rate constants, is required to achieve high-flux transport.”



### 2.4.2 *Can Diffusion Alone Explain G-Actin Delivery to the Filopodial Tip?*

We first explored whether, and under which conditions, diffusion might be sufficient to supply barbed end actin polymerization processes in filopodia considering the work by others who investigated actin diffusion as a key mechanism in filopodia. For reasons of simplicity, our calculations do not consider filopodial elongation, but analyze conditions where retrograde flow and polymerization are in balance, thus maintaining filopodial shape, length, retrograde flow in a steady state. For our calculations we used the parameter values indicated in bold text in Table 2.1.

In short filopodia of 1–2  $\mu\text{m}$ , the concentration of free actin at the filament base is still sufficient to supply enough polymerization for filopodial extension to occur [36]. This is in agreement with (2.1) for estimating the approximate time required for a particle to diffuse over a given distance  $x$ , in an environment where its diffusion coefficient is  $D$

$$t \approx \frac{x^2}{q_i D} \quad (2.1)$$

**Table 2.1** Parameters and data regarding filopodia and actin

Notation	Meaning	Value	References
$L$	Filopodial length	24–55 $\mu\text{m}$	[2]
		0.03–0.15 $\mu\text{m}$	[35]
		1–10 $\mu\text{m}$	[43]
		10–20 $\mu\text{m}$	[52]
		3–10 $\mu\text{m}$	[56]
		<b>Here: 1–30 <math>\mu\text{m}</math></b>	
$N$	Number of filaments in the filopodial bundle	10–30	References in [36]
$C_0$	G-actin concentration at filopodial base	10 $\mu\text{M}$	[36]
$k_{\text{on}}$	Polymerization rate	10 $\mu\text{M}^{-1}\text{s}^{-1}$	[36]
		11.6 $\mu\text{M}^{-1}\text{s}^{-1}$	[60]
$N_0$	Number of filaments to support protrusion	13	[36]
$\eta$	Unit conversion factor	20	[36]
$\delta$	Half-size of actin monomer	2.7 nm	References in [43]
$D$	G-actin diffusion coefficient	4 $\mu\text{m}^2/\text{s}$	[35]
		<b>5 <math>\mu\text{m}^2/\text{s}</math></b>	[32]
$V_{\text{ret}}$	Retrograde flow rate	<b>70 nm/s</b>	[36]
		30–80 nm/s	[56]

Values selected for this chapter are shown in bold

In (2.1),  $q_i$  is 2, 4, or 6 depending on the number of dimensions ( $i = 1, 2$  or  $3$ ) [26]. Considering a linear displacement ( $q_i = 2$ ) and a diffusion coefficient of  $5 \mu\text{m}^2/\text{s}$ , a G-actin travels  $3.16 \mu\text{m}/\text{s}$ .

For filaments longer than a few micrometers, we can analyze concentration of free actin according to expression (2.2) mentioned in [36]:

$$C(x) = C_0 - \frac{C_0 x}{L(t) + (D\eta e^{N_0/N})/(k_{\text{on}}N)} \quad (2.2)$$

In (2.2),  $L(t)$  indicates filopodial length as a function of time, (i.e., considering filopodial elongation or shrinkage). Our work does not consider elongation, so we assume  $L(t) = L$  constant. Furthermore, we chose the filopodial length interval to cover for a wide range of natural filopodia (Table 2.1), although values between 10 and  $20 \mu\text{m}$  are more frequently observed [7]. Function  $C(x)$  is the G-actin concentration at a given distance between the filopodial base ( $x = 0$ ) and the filopodial tip ( $x = L$ ). Therefore, the free actin concentration at the tip of the filopodium is given by the function expressed in

$$C = C(L, N, k_{\text{on}}) = C_0 - \frac{C_0 L}{L + (D\eta e^{N_0/N})/(k_{\text{on}}N)} \quad (2.3)$$

This value allows for calculating how many actins reach the polymerization point  $N_p$  in scenarios generated by varying  $L$ ,  $N$ , and  $k_{\text{on}}$ . The chosen values are in the ranges reported in Table 2.1.

The key question is whether diffusion is sufficient to sustain polymerization in order to balance the actin-bundle retrograde flow ( $V_{\text{ret}} = 70 \text{ nm}/\text{s}$  in Table 2.1). To achieve this velocity, a polymerization frequency of 30 actins/s per filament in the bundle is required when considering that every new actin elongates a filament by  $\approx 2.7 \text{ nm}$  (Table 2.1). Therefore, in a bundle with  $N$  filaments,  $N_{\text{ret}} = 30N$  actins should be polymerized per second. This will be compared with the number of actins obtained from (2.3), to check if diffusion is enough to sustain F-actin retrograde flow.

At a G-actin concentration of  $10 \mu\text{M}$ , the polymerization rate per actin filament was reported to be  $0.3 \mu\text{m}/\text{s}$ , which means that 110 actins are polymerized in a single filament per second [45]. For a bundle with  $N$  filaments, the number of polymerizing actins  $N_p$  would be  $110N/\text{s}$ . By integrating this with expression (2.3), we have

$$NP = 110NC \quad (2.4)$$

as the number of actin polymerized at a given concentration  $C = C(L, N, k_{\text{on}})$ . The calculations were performed by the following routine:

- for  $L$  in range(min = 0.5, max = 30, step = 0.5):
  - for  $N$  in range(min = 10, max = 30, step = 1):
    - for  $k_{\text{on}}$  in range(min = 10, max = 12, step = 1):
      - Calculate  $C = C(L, N, k_{\text{on}})$ , following (2.3)

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 $N_{\text{ret}} = 30N$ 
 $N_p = 11NC$ 
If  $N_p < N_{\text{ret}}$ 
  Add one in the number of cases where  $N_p < N_{\text{ret}}$ 
else
  Add one in the number of cases where  $N_p \geq N_{\text{ret}}$  print 'Number of cases
where  $N_p < N_{\text{ret}}$  (in %)'

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Here  $N_p = 11NC$ , because the number of polymerized actins is directly proportional to the concentration of monomers. At a concentration of  $10 \mu\text{M}$ , 110 actins are polymerized per second on each filament, providing 11 actins/s at  $1 \mu\text{M}$ . The expression (3) yields  $C \rightarrow C_0$  when  $L \rightarrow 0$ , ensuring that  $N_p = 110N$  for a concentration close to that at the base of filopodia.

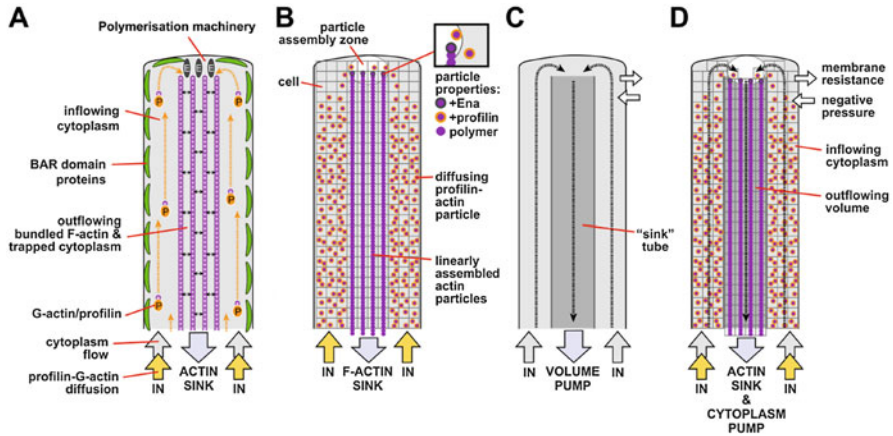
Using this algorithm in combination with the values given in Table 2.1, we obtain that of all cases the polymerization does not supply retrograde flow in 90.32 %. In comparison, when setting the filopodial length interval to  $L \in [0.5, 2] \mu\text{m}$ , diffusion seems ineffective in just 15 % of cases. This result suggests that diffusion alone is not sufficient in many scenarios, especially when reaching filopodial lengths beyond  $1.5 \mu\text{M}$ , and when  $N$  is greater than 21.

Other reports agree with our view. For example, Monte Carlo simulations were used to investigate G-actin translocation during protrusion of the leading edge leading to the conclusion that diffusion alone was insufficient [62]. The use of compartmental and molecular stochastic models to study actin motion by diffusion concluded that filopodia would reach a steady state length of as little as  $\approx 1 \mu\text{m}$  because the transport flux of G-actin monomers continuously diminishes as the tube becomes longer [17]. Also work on filopodia-like acrosomal processes of sperm found that the kinetics of diffusion-limited actin polymerization were not sufficiently rapid to account for the observed acrosomal elongation dynamics [42].

### 2.4.3 An Alternative Approach

The above calculations show that diffusion alone is, in general, not enough to supply the amount of G-actin needed to sustain the observed rates of polymerization and backflow. As one compensatory mechanism, Zhuravlev and colleagues proposed active motor-driven transport of G-actin [61], but there is hardly any experimental proof for this hypothesis. Therefore, we propose in the sequel a modeling approach which integrates a number of very different physical and chemical processes within filopodia (Fig. 2.3a): diffusion of actin building blocks, support-factor aided polymerization at the filament tips, as well as cytoplasmic flow driven by the forces caused by the displacement of actin filaments towards the filopodial base.

The idea of protein-mediated facilitation of polymerization was already explained in Sect. 2.2.1. Here, we briefly explain the concept of cytoplasmic flow. Thus, F-actin filaments at the core of the filopodium are constantly flowing backwards from the tip towards the cell through disassembly processes occurring



**Fig. 2.3** Cartoon models of filopodial dynamics. (a) Biological model: in cells, actin bundles are pulled out of filopodia from their minus-ends (ACTIN SINK) which is compensated through Ena/VASP-mediated (E) plus-end polymerization requiring supply (yellow arrows) with profilin (P)-bound G-actin (same symbols as explained in Fig. 2.1). Filopodial membranes are stabilized by BAR domain proteins. (b–d) Mathematical/computational models: (b) A model of diffusion and polymerization: the filopodium is subdivided into a coordinate system within which actin particles (magenta dots) undergo Brownian movement, diffusion, and assembly processes; to reflect contributions by regulatory proteins, actin particles are equipped with profilin- or Ena/VASP-bound properties (orange or brown circles; see close-up top right). (c) Flow model: filopodia are represented by a tube-in-tube constellation where volume (actin filaments with potentially trapped cytoplasm) flows out of filopodia, driven by a pump at the base of the inner tube, causing compensatory inflow of cytoplasm. (d) Combinatorial model: the coordinate system becomes dynamic reflecting the circulating cytoplasm flow from (c); actin particles with different properties (as in b) can diffuse and polymerize within this dynamic context, thus combining cytoplasmic flow, diffusion, and regulator-mediated polymerization

within the cell (Fig. 2.3a). This causes loss of volume in the filopodial tip which comprises the actin filaments, their hydration, other attached proteins, and perhaps even cytoplasm trapped in between the tightly packed actin filaments. If this volume loss is combined with sufficiently resistant membrane structure to prevent membrane collapse (open arrow in Fig. 2.3c), this would generate a negative pressure that needs to be compensated for by incoming cytoplasm to prevent cavitation.

Indeed filopodia seem to display such membrane rigidity provided by a class of proteins containing BAR (Bin-Amphiphysin-Rvs) domains (Fig. 2.3a) [30, 53, 54]. Given therefore a relatively stable shape of filopodia, the “outflow” of volume can be expected to drive a compensatory influx in the space between actin bundle and cell membrane towards the tip of the filopodium (Fig. 2.3c). The inflowing volume should be a mixture of cytosol (colloidal water) and G-actin molecules where the latter are still free to diffuse (Fig. 2.3d). At the tip of the filament the mixture-flow bends in the direction of the polymerization points, guided by the molecular organization around it, where the diffused G-actins are re-arranged

through polymerization into the backflowing filament bundle. The bending flow might even produce outward forces in the membrane that could further help sustain its form.

## 2.5 A Model for Filopodial Dynamics

### 2.5.1 *Principal Thoughts About Strategic Choices*

Three processes are central in the above description: diffusion, guided polymerization, and cytoplasmic flow. With polymerization being a chemically reactive process, we have a diffusion–reaction system with advection. In principle, there are several standard models from several mathematical disciplines which can describe such processes.

However, the mathematical modeling approaches to implement advection dynamics are very different from, and complementary to, those required by reaction–diffusion. Despite its hydro-dynamical elegance, the alternative approach above, that suggests a reorganization of particles within a flowing cytosol, cannot arise under the commonly used diffusion perspective because cytosol displacements are disregarded and only diffusive movements are represented. A new starting point is needed to suggest the models and observations needed to test it.

Furthermore, setting the standard equations for reaction, diffusion, and advection *per se* down as a model for filopodial dynamics is challenging, because they were developed based on very basic principles of homogeneity, uniformity, and isotropy, and the substances that react or drift are supposed to be present at any point of the domain. However, filopodia are anything else than isotropic or uniform. Different processes are predominant in very distinct regions of the filopodia and, thus, different equations should be used in distinct subregions of the model’s domain. For example, the standard equations allow, indeed enforce, actin reactions to take place anywhere in the filopodium and consider actin molecules as uniformly charged spheres, hampering the representation of what we know about protein-aided polymerization reactions which occur only at the plus-end of each filament. Furthermore, filopodia are bounded by (1) the moving cell membrane and (2) a rather unspecified surface at the bottom of the protrusion, and (3) further sub-domains are formed by the dynamic flow of distinct molecule classes: the backflowing actin bundles versus the (laminar) advection outside them. Therefore, the geometrical boundaries of each sub-domain cannot be determined in advance, as they result from molecular dynamics. Taking into consideration that we need to discretize the equations to perform simulations and numerical experiments, and that we are dealing at the very validity limit of continuous flow models [29], our chance of getting close to helpful and interesting solutions in this way is not very likely.

Based on these considerations, we prefer therefore computational models based on both mathematical and biological knowledge and tailored to what is known to

happen in each sub-domain of a filopodium. We consider here the combined use of two computational methods. First, the finite volume discretization with moving elements method, based on standard models of laminar flow and discretization methods which can track changes in the sub-domain geometry [13]. Second, the particle-in-cell method (PIC) relating to reaction–diffusion equations. This method can be used to model stochastic processes and simultaneously represent the rigid motion of the F-actin filament bundle, simply by considering transitions to be deterministic and remaining in a direction given by the central axis of the cylindrical portion of the filopodium.

### 2.5.2 *Modeling F-Actin Polymerization and Diffusion*

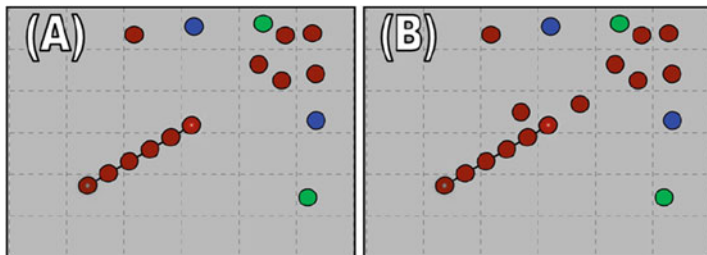
The PIC method we chose is a numerical technique that deals with problems where a fluid can be seen as particles scattered in a field described by a mesh, cf. [18, 48]. Every grid cell has a sufficiently large quantity of particles interacting with each other, carrying information about its own position and physico-chemical properties. PIC exhibits a widespread usage in computer simulation of plasma physics, gases, or other fluids composed of particles with high kinetic energy. It seems an efficient strategy to simulate the two-phase mixture here described.

Filopodia contain a collection of interacting particles and the cytosol. By particles we mean G-actin, F-actin, and ABPs, i.e., the key factors that interact and regulate the entire system. They are placed over a background field formed by the cytosol fluid or cytoplasm. Our model domain is an environment that involves a multi-scale fluid observation, in order to consider relevant, microscopic, and physical phenomena that bear influence on macroscopic properties of fluids.

In our chosen PIC model, each particle’s position is updated in response to system stimuli, such as fluid dragging, collision with other particles, or chemical reactions. For example, polymerization processes are triggered by the proximity of G-actins with the tip of F-actin bundles to which they bind. In this regime, distance can be used as a priority-parameter to decide which molecule polymerizes (Fig. 2.4).

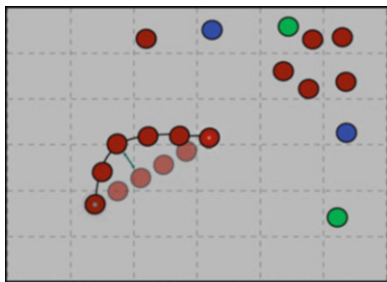
In addition, the position-tracking of particles permits to measure deformations through observation of displacements of F-actin position (Fig. 2.5). This information will be relevant in future analyses, for example, when incorporating forces, F-actin buckling, and membrane resistance.

In our preliminary simulations, particles move in Brownian motion through a 2D domain, and we observe G-actin concentration depletion in the area around a polymerization point (red dot in Fig. 2.6). This is an expected behavior since G-actins are consumed by polymerization and Brownian motion of other particles is not efficient enough to fill the vacant spaces.

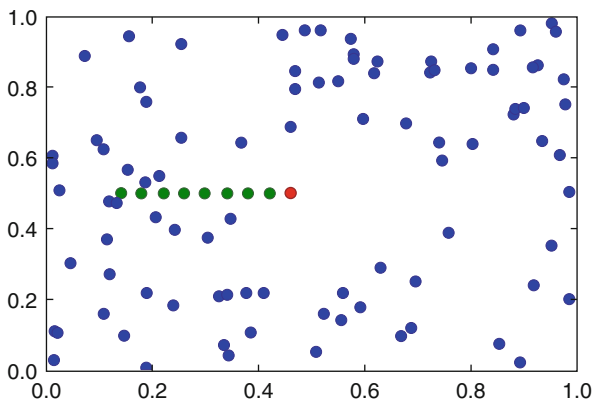


**Fig. 2.4** Schemes to represent possibility of particle interactions in our PIC simulations. (a) Several particles can be moving within same tiles (b) If a G-actin is in the same tile of polymerization point, it can be polymerized

**Fig. 2.5** Deformation of the filament measured through changes in particle positions



**Fig. 2.6** Particles (G-actins, blue) moving in Brownian motion, F-actins in green with the polymerization point (red dot) from where these filaments elongate. Note the decreasing G-actin concentration around the polymerization point



### 2.5.3 Modeling Cytosolic Flow as a Means to Drive Passive Transport of G-Actin

In order to investigate how G-actins are delivered to the polymerization points, we must consider physical properties of cytosol and fluctuations in the concentration of G-actins and other molecules throughout the domain. Therewith, we analyze cellular compensatory mechanisms for replacing the molecules consumed by polymerization, subject to the principle of mass conservation. Cytosol has a

colloidal-water constitution which, in first approximation, leads to considering it as an incompressible and viscous fluid and modeling its motion by Navier–Stokes equations for incompressible fluid flow [29],

$$\rho \left( \frac{\partial \mathbf{U}}{\partial t} + (\mathbf{U} \cdot \nabla) \mathbf{U} \right) = -\nabla p + \mu \mathbf{U} + \mu \nabla^2 \mathbf{U} + F \quad (2.5)$$

$$\frac{\partial \rho}{\partial t} + \nabla \cdot (\rho \mathbf{U}) = F_m \quad (2.6)$$

Here  $\mathbf{U}$  stands for the velocity vector,  $\rho$  for the fluid density,  $\mu$  for the dynamic viscosity,  $p$  for the hydrostatic pressure,  $F$  for the source of movement, and finally  $F_m$  for the source of mass. Considering filopodia as a system where fluid velocities are low, with high viscosity, and very small length-scales, Navier–Stokes above Eqs. (2.5)–(2.6) can be simplified and written as:

$$\nabla p - \mu \nabla^2 \mathbf{U} = F \quad (2.7)$$

$$\nabla \mathbf{U} = F_m \quad (2.8)$$

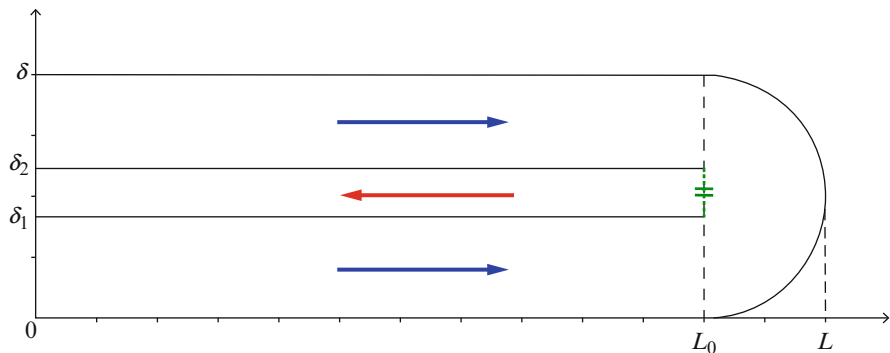
taking into account that  $\rho = \text{constant}$ , due to fluid incompressibility. Flows with these characteristics are called Stokes flows and Eqs. (2.7)–(2.8) are known as Stokes equations.

At this point, the fluid can be analyzed through a macroscopic approach, i.e., in a laminar flow with a certain concentration of G-actins in suspension, since the latter are supposed to be passively transported by the cytosol and do not affect its flow. This scenario is based on assumptions described in previous sections: the volume removed from the filopodia tip induces a hydrostatic pressure, thus leading to the cytosol displacement.

The conditions and processes we seek to investigate with the tools under development include the rules underlying G-actin motion, hydrostatic pressure, and membrane resistance. Aiming to enforce mass conservation inside the filopodia, which is a critical aspect of our approach, we have decided to discretize the model flow equations with the finite volume method. Notably, PIC can be coupled with finite volume laminar flow giving an integrated two-phase representation of an entire system as a dynamic fluid, to study the reorganization of the actin-phase into filaments at molecular scales. Within a neighborhood of the polymerization points, the two methods merge by superposition: the PIC method determines the movement of G- and F-actins relative to the volume elements, and the finite volume algorithm drives the displacement and deformation of these volume elements. Volume elements trapped within the F-actin filament bundle move then with the filaments.

The domain of our model mimics filopodia interior and will initially be two-dimensional for implementation tests. The scheme in Fig. 2.7 represents a filopodium and a bundle of actin filaments inside, where red arrow means retrograde flow. The cytoplasmic fluid is pumped from lamellipodia in  $x = 0$ ,





**Fig. 2.7** Filopodia fluid motion scheme

for  $y \in [0, \delta_1) \cup (\delta_2, \delta]$ . Filopodium is also bounded by the membrane at  $x = L$ . Actin polymerization occurs at  $x = L_0$  where  $y \in [\delta_1, \delta_2]$ . This region is the inset of a tube that represents F-actin filament bundle and drives actins out of filopodia, acting as a sink.

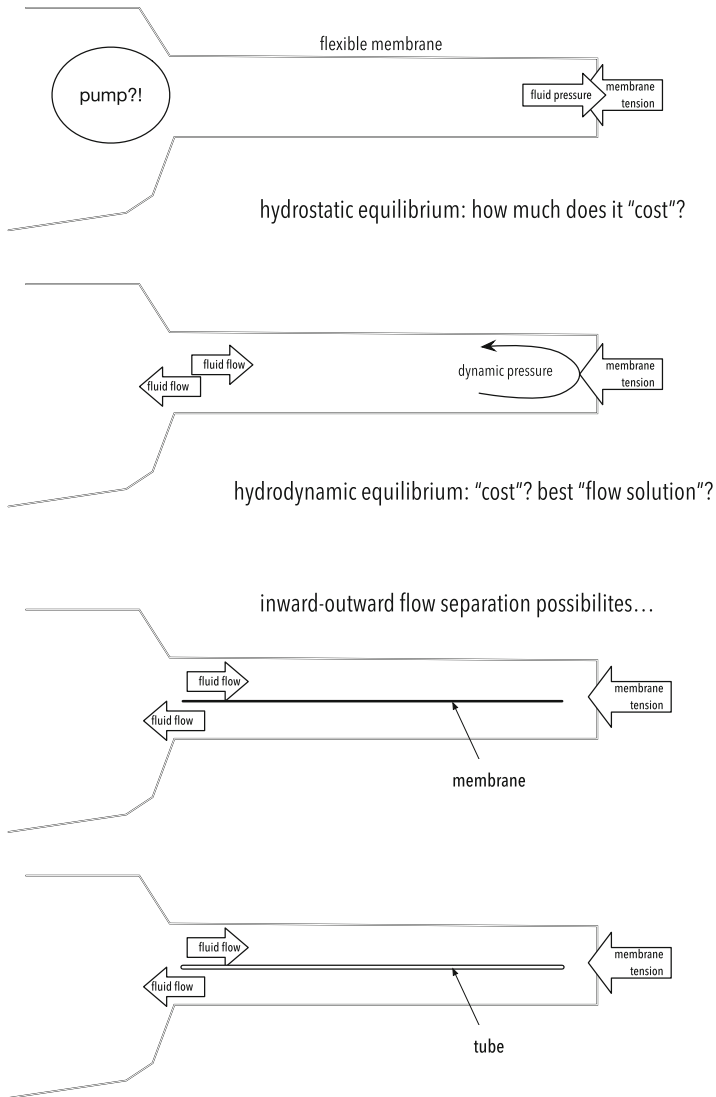
### 2.5.4 Model Validation

Model validation is a long-term project which relies on the confidence we gain from solving questions and explaining biological measurements with our model. Nevertheless, there are series of immediate experiments that can be undertaken to check both the model's conceptual soundness and its implementation.

We have seen in Sect. 2.5.2 that the PIC model represents well the diffusion of G-actins, the formation of filaments, and their almost rigid-like motion along a line. Computational models for laminar flows based on finite volumes are well known, as well as their validation. The steps below address the coupling of both algorithms and the representation of characteristics relevant for biological enquiries and the special filopodia geometry.

First, we need to verify basic aspects: mass conservation, soundness of the flow bending at the tip, coupling of advective currents with the polymerization points, and the return of G-actins by the cytosolic inward flow. Furthermore, we need to verify if the superimposition of both models retains properties relevant for the biological problem: does it (1) provide enough actins at the polymerization points? (2) reduce the flow when polymerization stops? (3) represent elongation and retraction of the filopodia? and so on.

Moreover, the model can be used to perform tests that provide data supporting the approach proposed, like those suggested in Fig. 2.8. The results of numerical (virtual) experiments of this type provide data in favor or against the proposed approach.



**Fig. 2.8** Biological Questions—what is the most efficient way of sustaining the cell membrane in protrusions, and providing enough actins to keep the polymerization rate?

## 2.6 Conclusions

This chapter presents a novel approach to the description of the flow of matter inside filopodia, adding advection of the cytosol to the diffusion of molecules suspended or dissolved within it. Proposing this advection is justified by the biological knowledge that volume (actin, attached proteins, and cytosol) is withdrawn from the filopodia,

providing a pump mechanism for compensatory inflow. This research is in its infancy and a lot of open questions lay ahead, besides those related to model validation. These open questions include: (1) relations between the number of filaments in the bundle and several aspects, like flow velocity, G-actin concentration, elongation–retraction of the protrusion, etc; (2) the mechanical effects or the flow over the membrane throughout the filopodia; and (3) how the outward movement of the filament bundle affects the laminar inward flow. We are working towards joining the PIC and the finite volume algorithms and hope to be addressing these intriguing questions in the near future and couple them up with imaging experiments in *Drosophila* growth cones. However, our ultimate goal is to understand how this flow apparatus can be regulated and controlled to yield all behavior we observe in filopodia.

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